

# SMALL FIELDS DOSIMETRY: OUTPUT FACTORS AND CORRECTION FACTORS DETERMINATION FOR AN ELEKTA AXESSE MEDICAL LINAC EQUIPPED WITH CIRCULAR CONES

A. Girardi<sup>1</sup>, C. Fiandra<sup>2</sup>, E. Gallio<sup>3</sup>, F.R. Giglioli<sup>3</sup> and R. Ragona<sup>2</sup>

<sup>1</sup>Universitair Ziekenhuis Brussel, Department of Radiotherapy, Brussels, Belgium

<sup>2</sup>University of Torino, Department of Oncology, Radiation Oncology Unit, Torino, Italy.

<sup>3</sup>Azienda Ospedaliero - Universitaria Città della Salute e della Scienza, Medical Physics Unit, Torino, Italy.

1<sup>st</sup>

EUROPEAN  
CONGRESS OF  
MEDICAL  
PHYSICS



September 1-4, 2016  
Eugenides Foundation  
Athens-Greece

# IAEA/AAPM formalism for small field dosimetry

$$\Omega_{Q_{clin}, Q_{msr}}^{f_{clin}, f_{msr}} = \frac{M_{Q_{clin}}^{f_{clin}}}{M_{Q_{msr}}^{f_{msr}}} \times k_{Q_{clin}, Q_{msr}}^{f_{clin}, f_{msr}}$$

$f_{msr}$ : machine-specific reference field

$f_{clin}$ : clinical field

The correction factors  $k$  can be determined through:

- primary standard
- passive dosimeter (alanina, radiochromic films)
- MonteCarlo simulations

# Purpose

–to determine OUTPUT FACTORS  $\Omega$  for several active detectors and one passive dosimeter (Gafchromic EBT3 films) for an Elekta Axesse with circular collimator (diameter 5 – 30 mm)

–to determine the CORRECTION FACTORS  $k$  for the active detectors for comparison with films

$$\Omega \frac{f_{clin}, f_{msr}}{Q_{clin}, Q_{msr}} = \frac{M \frac{f_{clin}}{Q_{clin}}}{M \frac{f_{msr}}{Q_{msr}}} \times k \frac{f_{clin}, f_{msr}}{Q_{clin}, Q_{msr}}$$

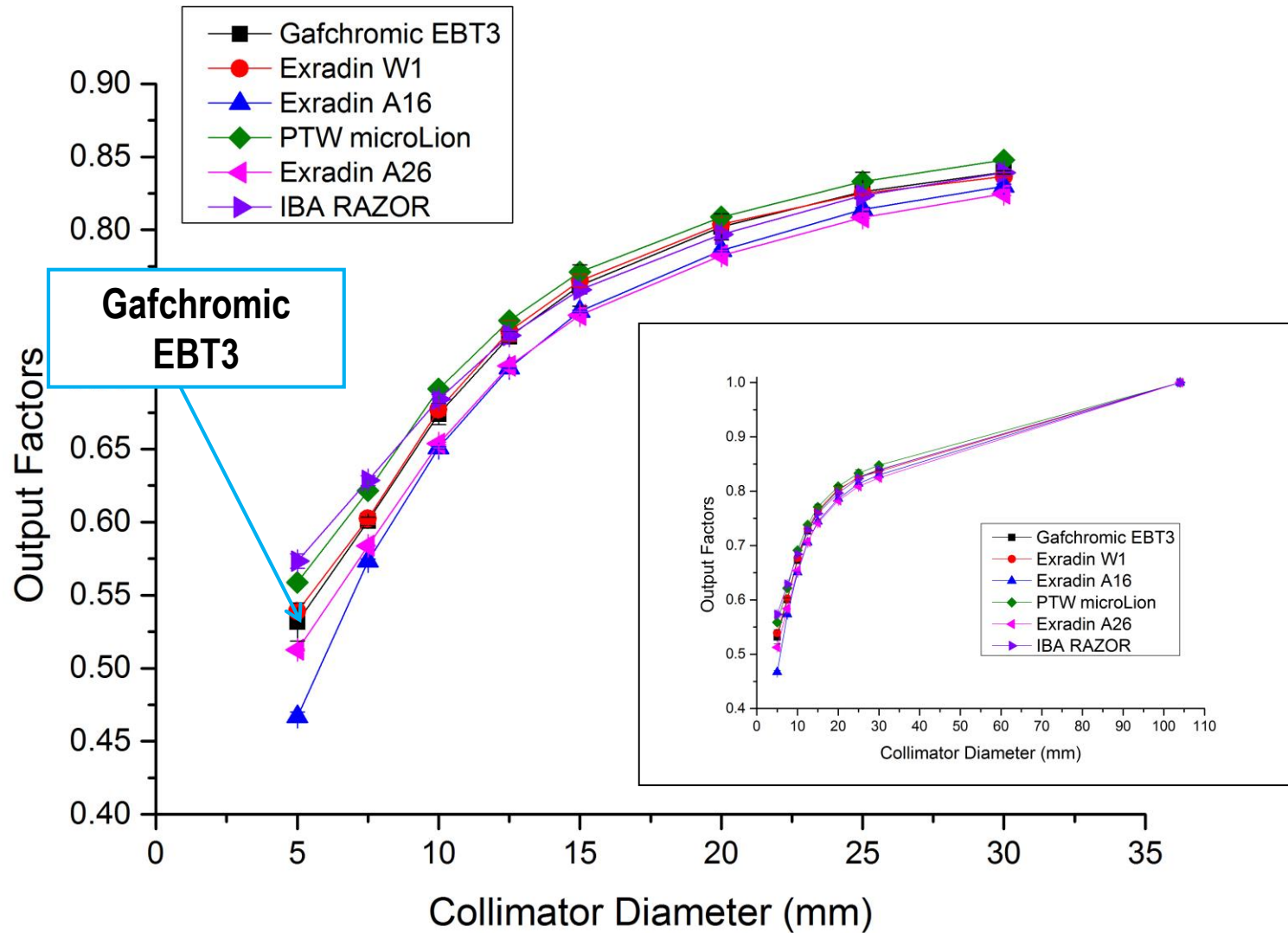
# Detectors Overview

Detector	Density	Active volume	Additional components
Gafchromic EBT3	1.1 g/cm <sup>3</sup>	72 dpi → voxel size ≈ 0.080 mm <sup>3</sup>	Polyester
Exradin A16	0.0013 g/cm <sup>3</sup>	7 mm <sup>3</sup>	Shonka C-552
Exradin A26	0.0013 g/cm <sup>3</sup>	15 mm <sup>3</sup>	Shonka C-552
Exradin W1	1.05 g/cm <sup>3</sup>	3 mm <sup>3</sup>	Optical fiber
PTW microLion	0.69 g/cm <sup>3</sup>	1.7 mm <sup>3</sup>	Graphite electrode
IBA Razor	2.33 g/cm <sup>3</sup>	0.006 mm <sup>3</sup>	ABS plastic + epoxy

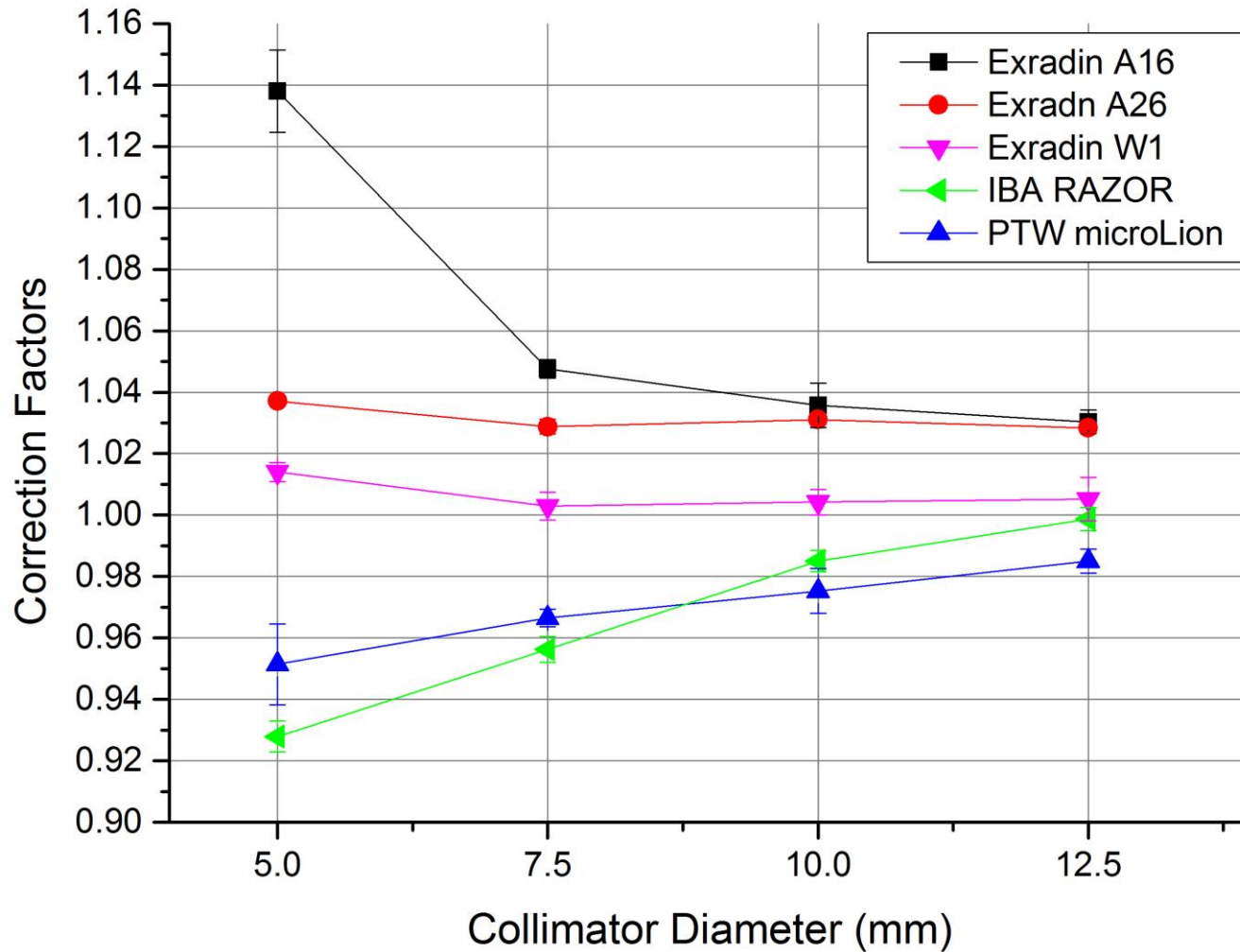
# Measurements geometry

- Active detectors in PTW MP<sup>3</sup> phantom (axially)
- SSD = 90 cm, depth = 10 cm
- MLC Collimation upstream of the cone:  
 $f_{\text{MLC}} = 4 \times 4 \text{ cm}^2$
- Dosimetrical positioning (Trifix tool ) relative to 5 mm cone
- $f_{\text{msr}} = 10.4 \times 10.4 \text{ cm}^2$  ,  $d(f_{\text{clin}}) = 5 \div 30 \text{ mm}$
- Films placed in Solid Water phantom
- Measurements repeated three times for each field

# Results



Detector	Behavior in small fields	5 mm cone	7.5 mm cone	10 mm cone
Exradin A16	Underestimation	- 12 %	- 5 %	- 3.5 %
Exradin A26	Underestimation	- 3.7 %	- 2.8 %	- 3 %
Exradin W1	Very close to films	+ 1.5 %	k = 1	k = 1
PTW microLion	Overestimation	+ 5 %	+ 3.5 %	+ 2.5 %
IBA Razor	Overestimation	+ 8 %	+ 4.6 %	+ 1.5 %





# Correction factors interpretation

$$k_{\frac{f_{clin}, f_{msr}}{Q_{clin}, Q_{msr}}} = P_{vol} \times P_{fl} \cdot P_{spec}$$

Azangwe et al., Med  
Phys 2014

- ❖  $p_{vol}$ : volume averaging correction
- ❖  $p_{fl} \cdot p_{spec}$ : perturbation detector correction  
Medium density  $\neq 1 \text{ g/cm}^3$

Scott et al., Phys. Med. Biol. 57 (2012): “*The variation at small field sizes is shown to be due to differences between the densities of detector active volumes and water, rather than differences in atomic number.*”

# Conclusions

Using an accuracy level of 2% (Underwood et al. Phys. Med. Biol. 60,2015):

- Exradin W1 does not need corrections, even for collimator diameter below 10 mm
- IBA RAZOR can be used to measure 10 mm cone without corrections
- Other detectors should be not used below 10 mm diameter cone without correction factors